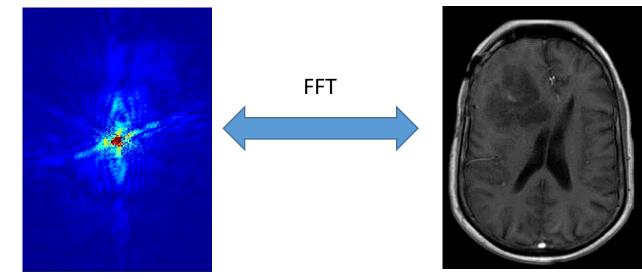
### Direct model-based reconstruction for high-resolution whole-brain DCE-MRI

Yi Guo MHI pitch presentation



#### Magnetic Resonance Imaging (MRI)

- MRI is a noninvasive medical imaging tool to produce 3D images using multiple magnetic fields.
- Dynamic Contrast Enhanced (DCE) MRI acquires a series of images to capture the dynamic changes during a contrast injection
  - Essential to evaluate brain tumor and other abnormality



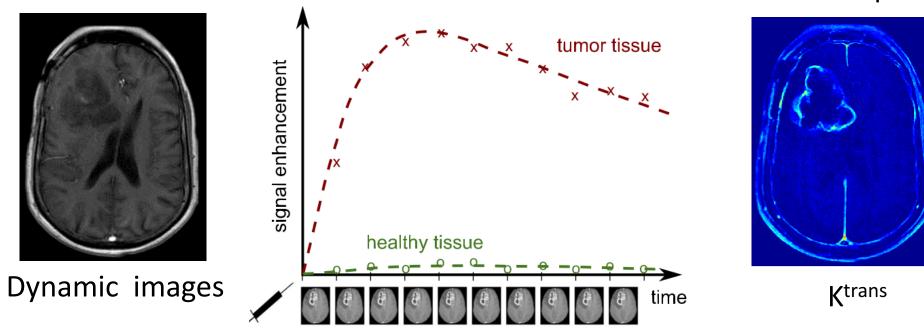
Dynamic Contrast Enhanced MRI

Nyquist sampling in MRI raw data space (k-space)



### Tumor evaluation using DCE-MRI

 Tumor severity evaluation: important pathological information from tracker-kinetic (TK) maps (K<sup>trans</sup>, v<sub>p</sub>, v<sub>e</sub> etc.).





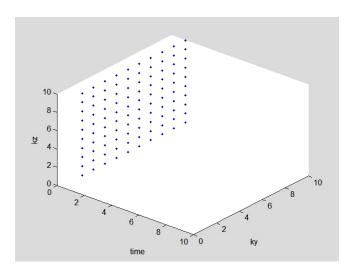


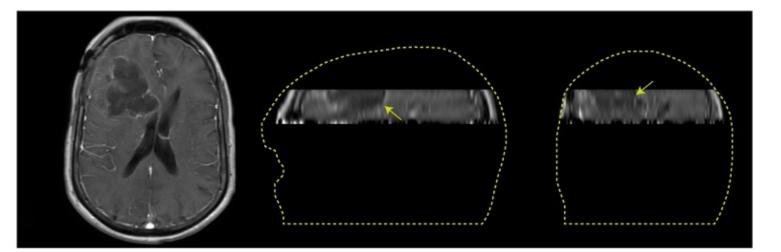
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# Limited coverage and resolution for conventional DCE-MRI

5s temporal resolution, Nyquist sampling (used clinically)
-> 7 slices, 0.9x1.3x7.0 mm<sup>3</sup> in plane resolution





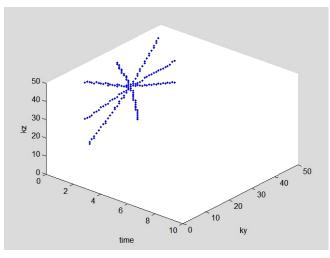
Cartesian Nyquist sampling

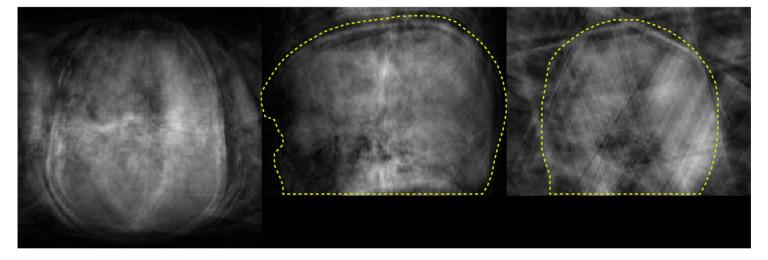
Limited coverage and resolution



#### Under-sampling reconstruction

- 5s temporal resolution, 30x undersampling
  - -> 100 slices, 0.9x0.9x1.9 mm<sup>3</sup> in plane resolution





Cartesian Golden-angle radial sampling at 30x

Zero-padded images

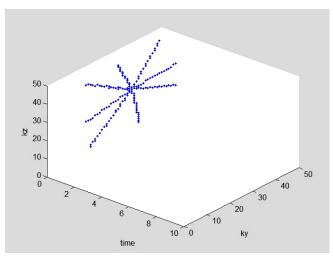


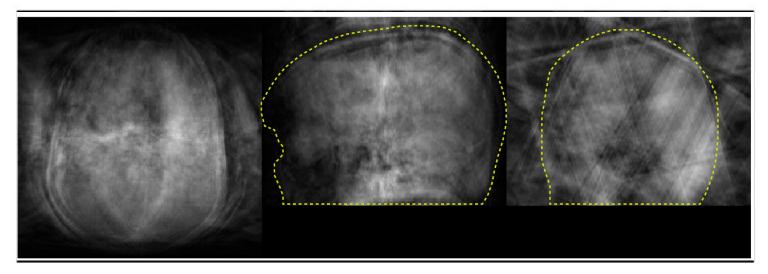
#### Under-sampling reconstruction

• Constrained reconstruction:

$$x = \underset{x}{\operatorname{argmin}} \| y - F_u Sx \|_2^2 + \frac{1}{2} \| Vx \|_1 + \frac{1}{2} \| TVx \|_1 + \frac{1}{3} \| -x \|_1$$
[1]

Spatial and temporal sparsifying transform



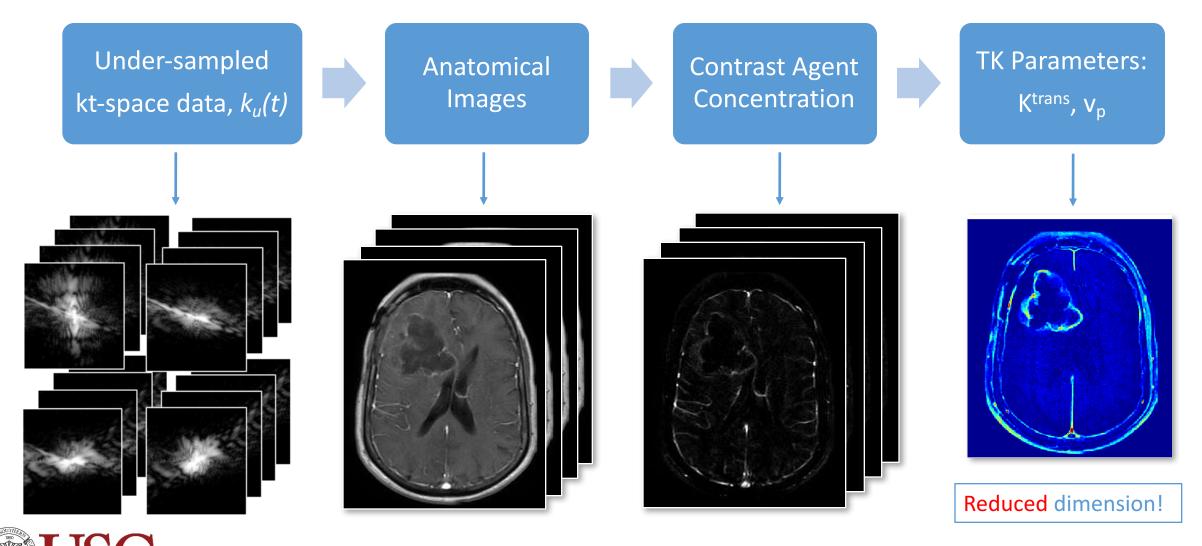


Cartesian Golden-angle radial sampling at 30x

Rezerstpacted images Whole-brain coverage



#### Indirect estimation of TK parameter maps

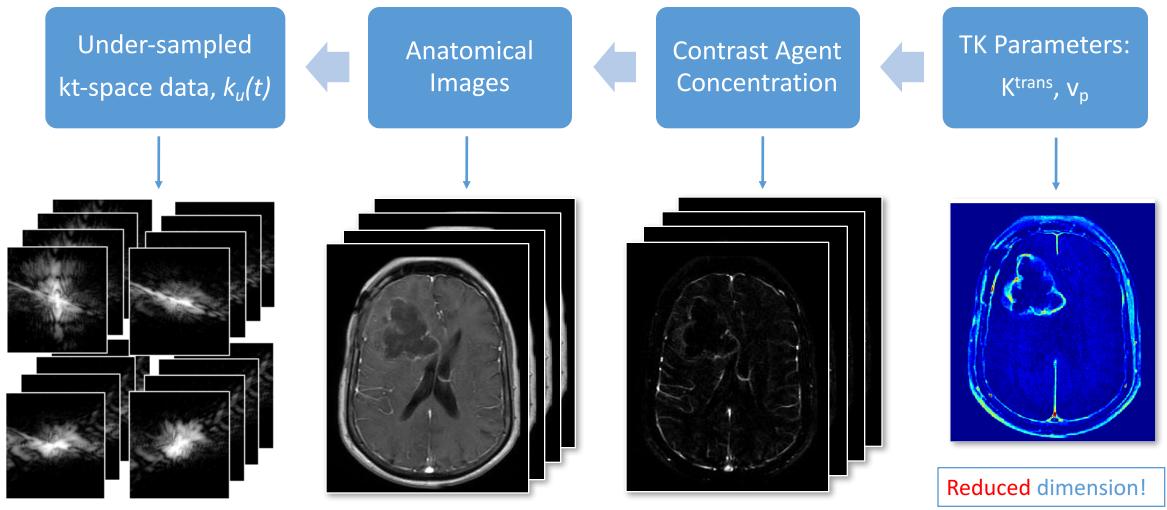


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### Forward modelling of TK parameter maps



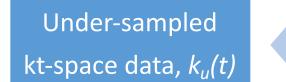


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### Forward modelling of TK parameter maps



Anatomical Images Contrast Agent Concentration TK Parameters: K<sup>trans</sup>, v<sub>p</sub>

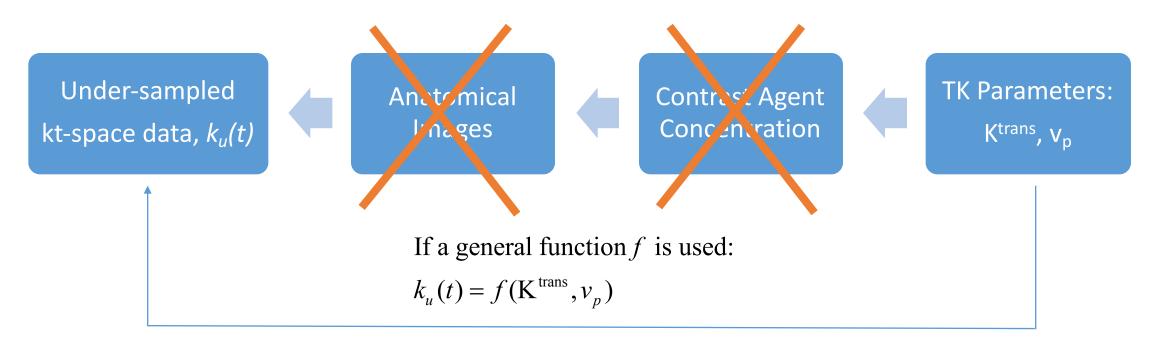
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#### Model-based direct estimation



Can sovle PK maps with an optimization problem:

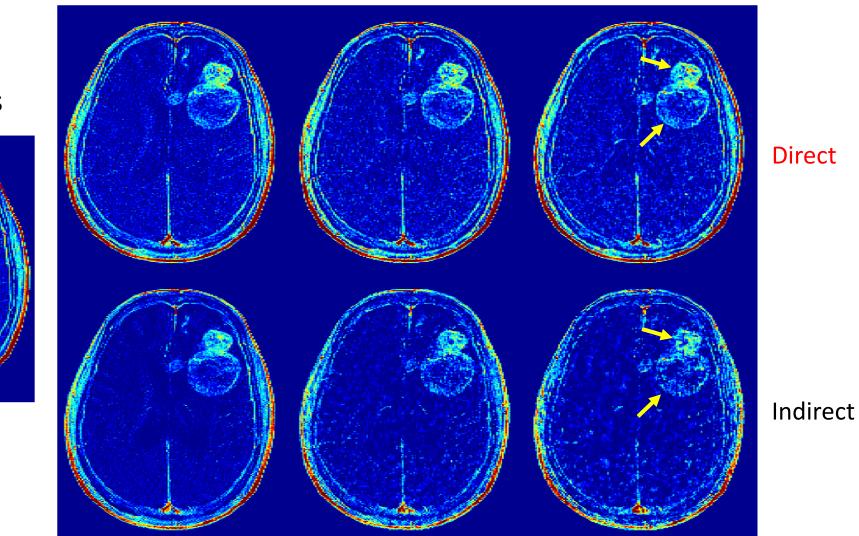
 $(K^{trans}, v_p) = \underset{K^{trans}, v_p}{\operatorname{argmin}} \| k_u(t) \quad f(K^{trans}, v_p) \|_2^2$ 

An efficient gradient-based I-BFGS method is used to solve the optimization problem



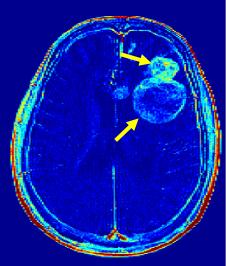
#### Up to 100x in retrospective study

20x



60x

K<sup>trans</sup> maps



Fully sampled



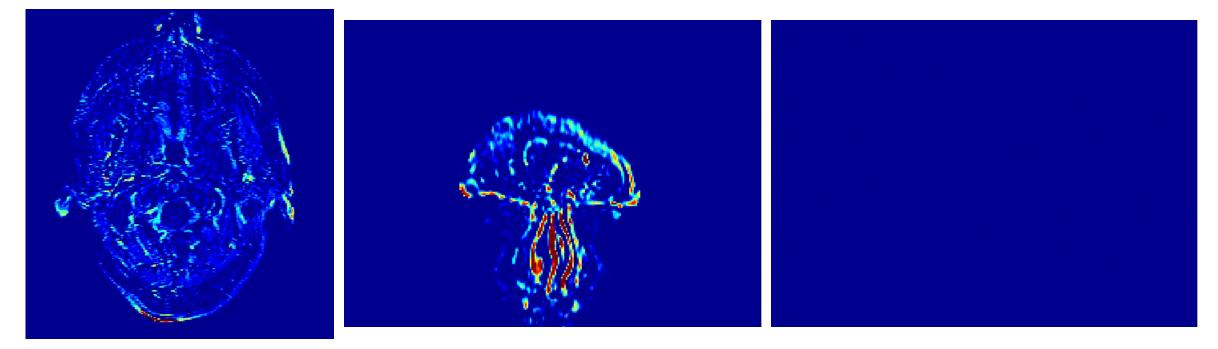


100x



## Whole-brain TK maps by model-based direct reconstruction

#### K<sup>trans</sup> maps



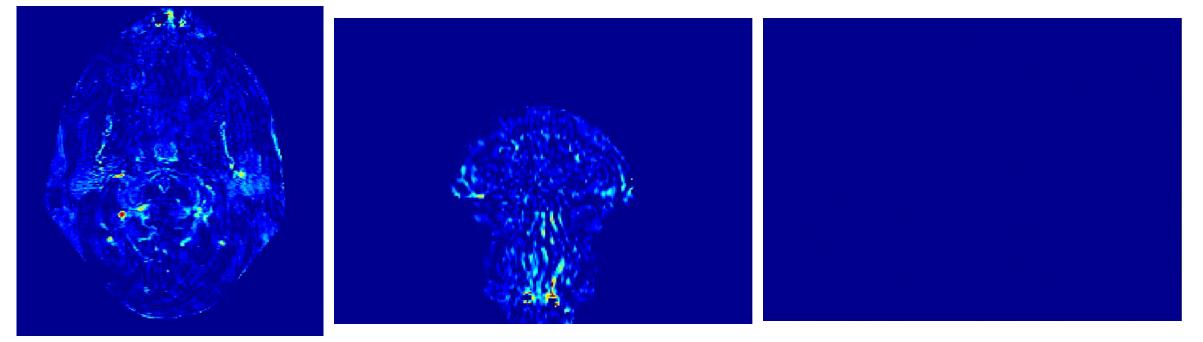
**Yi Guo,** et al. Direct Estimation of Tracer-Kinetic Parameter Maps from Highly Under-sampled Brain DCE-MRI, *Magnetic Resonance in Medicine* (early view)



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# Whole-brain TK maps by model-based direct reconstruction

#### V<sub>p</sub> maps



**Yi Guo,** et al. Direct Estimation of Tracer-Kinetic Parameter Maps from Highly Under-sampled Brain DCE-MRI, *Magnetic Resonance in Medicine* (early view)

